

REVIEW

Open Access



The in situ efficacy of whole room disinfection devices: a literature review with practical recommendations for implementation

Caroline M. van der Starre, Suzan A. J. Cremers-Pijpers, Carsten van Rossum, Edmée C. Bowles and Alma Tostmann*

Abstract

Background: Terminal cleaning and disinfection of hospital patient rooms must be performed after discharge of a patient with a multidrug resistant micro-organism to eliminate pathogens from the environment. Terminal disinfection is often performed manually, which is prone to human errors and therefore poses an increased infection risk for the next patients. Automated whole room disinfection (WRD) replaces or adds on to the manual process of disinfection and can contribute to the quality of terminal disinfection. While the in vitro efficacy of WRD devices has been extensively investigated and reviewed, little is known about the in situ efficacy in a real-life hospital setting. In this review, we summarize available literature on the in situ efficacy of WRD devices in a hospital setting and compare findings to the in vitro efficacy of WRD devices. Moreover, we offer practical recommendations for the implementation of WRD devices.

Methods: The in situ efficacy was summarized for four commonly used types of WRD devices: aerosolized hydrogen peroxide, H₂O₂ vapour, ultraviolet C and pulsed xenon ultraviolet. The in situ efficacy was based on environmental and clinical outcome measures. A systematic literature search was performed in PubMed in September 2021 to identify available literature. For each disinfection system, we summarized the available devices, practical information, in vitro efficacy and in situ efficacy.

Results: In total, 54 articles were included. Articles reporting environmental outcomes of WRD devices had large variation in methodology, reported outcome measures, preparation of the patient room prior to environmental sampling, the location of sampling within the room and the moment of sampling. For the clinical outcome measures, all included articles reported the infection rate. Overall, these studies consistently showed that automated disinfection using any of the four types of WRD is effective in reducing environmental and clinical outcomes.

Conclusion: Despite the large variation in the included studies, the four automated WRD systems are effective in reducing the amount of pathogens present in a hospital environment, which was also in line with conclusions from in vitro studies. Therefore, the assessment of what WRD device would be most suitable in a specific healthcare setting mostly depends on practical considerations.

*Correspondence: alma.tostmann@radboudumc.nl

Unit of Hygiene and Infection Prevention, Department of Medical Microbiology, Radboud Center for Infectious Diseases (RCI), Radboudumc, Geert Grooteplein Zuid 10, 6525 GA Nijmegen, The Netherlands



© The Author(s) 2022. **Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>. The Creative Commons Public Domain Dedication waiver (<http://creativecommons.org/publicdomain/zero/1.0/>) applies to the data made available in this article, unless otherwise stated in a credit line to the data.

Keywords: Whole room disinfection, Automated room disinfection, Aerosolized hydrogen peroxide, Hydrogen peroxide vapour, Ultraviolet C, Pulsed-xenon ultraviolet, Disinfection, Decontamination, Hospital acquired infections, Infection prevention and control

Background

Hospitalized patients who have an infection with or are a carrier of a multidrug resistant micro-organism (MDRO), such as methicillin-resistant *Staphylococcus aureus* (MRSA), vancomycin-resistant *Enterococcus* (VRE) and multidrug resistant *Acinetobacter baumannii*, have to be cared for in isolation. After discharge of a patient with an MDRO, the patient room needs terminal cleaning and disinfection to eliminate the MDRO from the environment.

Terminal disinfection is often performed manually, which is labour intensive and prone to human errors. Errors can be made in the selection of the correct detergent, the formulation of the detergent in the correct concentration, the distribution of the product, and the adherence to the correct contact time [1–3]. This conventional way of disinfection therefore often does not eliminate all pathogens in a patient room [4–7]. Consequently, the risk for infection or carriage with the same MDRO for the next patient residing in such a patient room is at least two-fold but may even be greater than five-fold depending on the MDRO [8–10].

Automated ‘whole room disinfection’ (WRD) is a technology that can contribute to the quality of the terminal disinfection of patient rooms. WRD devices replace or add to the manual disinfection process by an automated process with a constant result. WRD still needs to be preceded by manual cleaning of the patient room, which is also common practice for manual disinfection.

Currently, there are four types of WRD devices that are used most frequently in a hospital setting. Aerosolized hydrogen peroxide (aHP) and H₂O₂ vapour make use of gaseous hydrogen peroxide. Ultraviolet C (UV-C) and pulsed-xenon UV (PX-UV) make use of ultraviolet radiation.

The efficacy of WRD devices is primarily assessed by its in vitro outcomes, which considers the logarithmic reductions of in vitro presence of pathogens after treatment with a WRD device. In vitro studies are performed in a controlled environment, where the investigated pathogen is cultured in specific quantities and treated with a standardized disinfection process. Therefore, in vitro evaluations may present the efficacy under ideal circumstances. Amongst the most frequently used types of WRD devices, H₂O₂ vapour has the highest in vitro efficacy, followed by UV-C.

In contrast to the in vitro conditions, the real-life settings in which WRD devices will be implemented, such as hospitals, present less optimal environments. The exact location and quantity of the pathogen is unknown and disinfection may be limited due to soiled surfaces. Additionally, WRD devices may not reach all areas of the patient room and efficacy may differ for the various kinds of surfaces. Furthermore, materials and medical equipment present in the room may not be suitable for or suffer from disinfection with e.g. UV-C or hydrogen peroxide. Therefore, the in situ efficacy may differ from the in vitro efficacy of WRD devices.

In this review we have summarized available scientific literature on the in situ efficacy of WRD devices in a hospital setting to get insight into the effect of WRD devices in real-life and less standardized settings. Therefore, we aim to describe the in situ efficacy of WRD devices in a hospital setting and how the in situ efficacy compares to the in vitro efficacy of such WRD devices. Moreover, we offer practical information concerning the WRD devices and provide recommendations for implementation.

Methods

This review is limited to the four types of WRD devices that are most frequently used in a hospital setting: aHP, H₂O₂ vapour, UV-C and PX-UV. The efficacy of these WRD devices has been investigated for common micro-organisms known to cause hospital-acquired infections or hospital outbreaks, being norovirus, *Acinetobacter*, carbapenemase-producing *Enterobacteriaceae* (CPE), extended spectrum beta-lactamase (ESBL) producers, MRSA, VRE, *Clostridium difficile* and *Candida auris*.

In addition to a summary of the available literature concerning the efficacy of the four types of WRD devices, this review also describes and assesses the features and practicalities of each type. Data was collected via literature and through interviews with experts in hygiene and infection prevention, both within our unit as from other Dutch hospitals.

Outcome measures

For in situ efficacy, a distinction was made between environmental and clinical outcome measures. The environmental outcome measure was defined as the difference in the microbial contamination before and after disinfection with a WRD device, expressed in the number of positively tested sites or rooms, or the number of colony-forming

Table 1 The initial and second search string as applied in PubMed in September 2021

| | |
|-------------------|--|
| | ("Acinetobacter"[tiab] OR "Norovirus"[tiab] OR "NoV"[tiab] OR "VRE"[tiab] OR "Vancomycin-resistant enterococc*" [tiab] OR "CPE"[tiab] OR "Carbapenemase-Producing Enterobacter*" [tiab] OR "MRSA"[tiab] OR "methicillin resistant <i>Staphylococcus aureus</i> " [tiab] OR "ESBL"[tiab] OR "Extended spectrum beta-lactamase"[tiab] OR "Candida Auris"[tiab] OR "C. auris"[tiab] OR "clostridium difficile"[tiab] OR "C. Difficile"[tiab] OR "Ebola virus"[tiab] OR "Lassa Virus"[tiab] OR "Marburgvirus"[tiab]) |
| AND | ("VHP"[tiab] OR "vaporized hydrogen peroxide"[tiab] OR "HPV"[tiab] OR "hydrogen peroxide vapor"[tiab] OR "aHP"[tiab] OR "aerosolized hydrogen peroxide"[tiab] OR "hydrogen peroxide vapour"[tiab] OR "PX-UV"[tiab] OR "pulsed xenon UV"[tiab] OR "UV-C"[tiab] OR "ultraviolet C"[tiab] OR "no-touch disinfection"[tiab] OR "whole room disinfection"[tiab] OR "automated room disinfection"[tiab]) |
| AND | ("hospital"[tiab] OR "ward"[tiab] OR "care institution"[tiab] OR "emergency room"[tiab] OR "facility"[tiab] OR "clinic"[tiab] OR "medical centre"[tiab] OR "nursing home"[tiab] OR "insitution"[tiab] OR "health centre"[tiab] OR "infirmary"[tiab]) |
| 1st search string | |
| 2nd search string | ("patient"[tiab] OR "patient room"[tiab]) |

units (CFUs) sampled in a patient room. This difference was converted to a percentage (increase or reduction in micro-organism). When both data regarding positive sites and rooms were reported in an article, data concerning positive sites were favoured as this information is more detailed. Only when no data concerning positive sites was available, data concerning the number of positive rooms was reported. The effect of disinfection as regarded in the studies performed for a certain micro-organism was summarized in a range of effect. In this range, data regarding the differences in the number of positive sites, rooms and CFUs were combined.

The clinical outcome measures was defined as the difference between the pre- and post-implementation period patient infection rate. This difference was converted to a percentage of increase or reduction. Both the microbial colonization or acquisition infection rates and the clinical infection rates were included in the clinical outcome measure.

The in vitro efficacy of the four WRD systems for the predefined micro-organisms was determined using a non-systematic literature search.

Search strategy

A literature search was performed in the medical database PubMed in September 2021. After the initial search, it was discovered that the terms "patient" and "patient room" yielded relevant articles as well. A second literature search was carried out with an adjusted search string. The initial and second literature search are presented in Table 1. Articles were primarily selected based on title and abstract. Subsequently, a final selection based on relevance of the full text was made.

Inclusion and exclusion criteria

Articles were applicable for inclusion if (1) they focussed on the decontamination of a (patient) room after discharge of a patient with one of the predefined micro-organisms; (2) the automated room disinfection was performed using aHP, H₂O₂ vapour, UV-C or PX-UV; (3)

it was published between January 2000 and September 2021 in a medical scientific journal; (4) it was available in English language; (5) it reported at least one of the environmental or clinical outcome measures of interest; and (6) applied WRD devices as a solitary intervention. Articles describing infections with micro-organisms other than those previously predefined or articles that did not specify included micro-organisms and articles that studied the effect of a bundle of interventions instead of the solitary effect of WRD were excluded from this review. The preparation of a patient room by cleaning (and decontamination) prior to disinfection with WRD were not regarded as a bundle of interventions, as cleaning is a crucial preparational element of WRD.

Data extraction

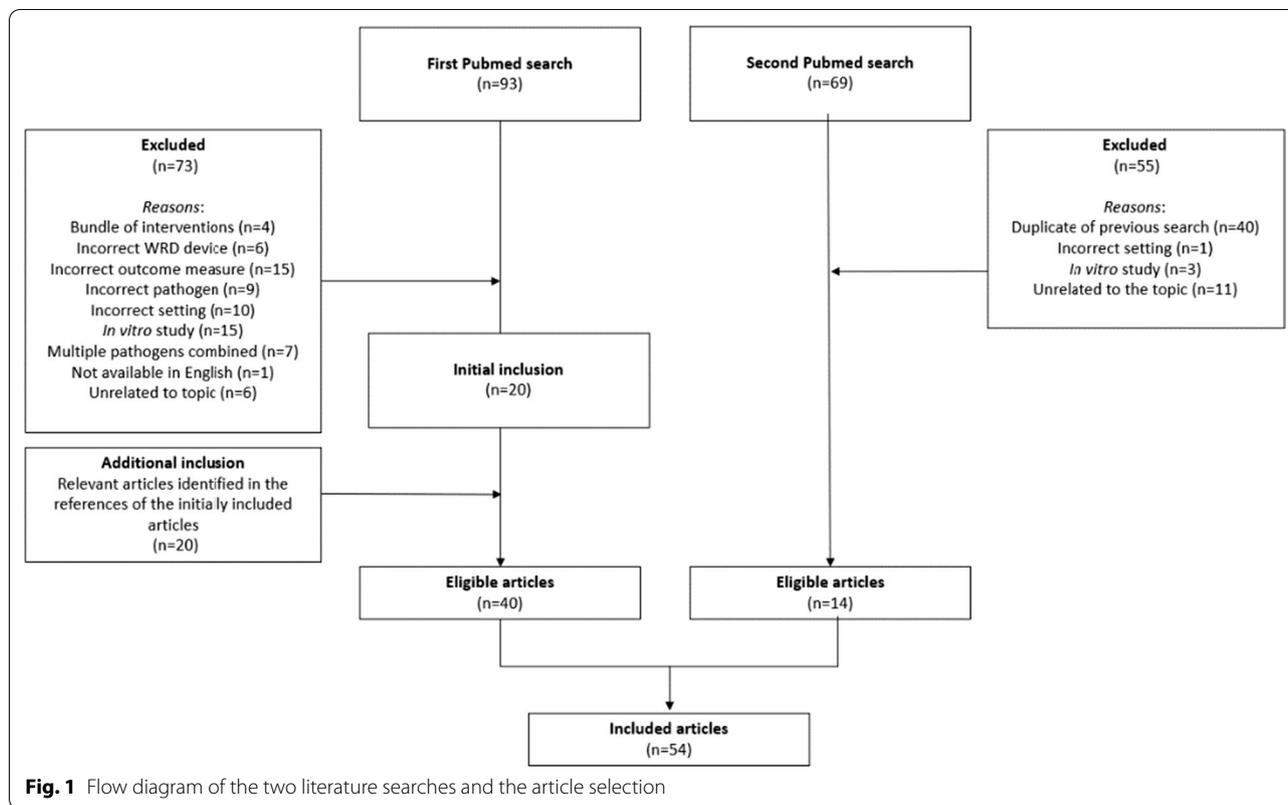
Data extracted from the included articles were: name of authors, year of publication, country in which the study was performed, setting (i.e. type of care institution in which the study was performed), study design, associated pathogen, type of WRD device and environmental or clinical outcome measure.

For each of the four types of WRD devices, a detailed description of the features, practicalities, in vitro and in situ efficacy is provided.

Results

Article selection

The initial search string yielded a total of 93 articles. After assessing these articles for eligibility, 73 articles were excluded. The main reasons for exclusion were having an incorrect outcome measure, an incorrect (or not hospital-related) setting or assessing in vitro instead of in situ efficacy. Through the assessment of references mentioned by the 20 eligible articles, another 20 relevant articles were included into the first literature search. A second search string yielded a total of 69 articles, of which 14 were eligible for inclusion. Based on the initial and second PubMed searches, a total of 54 articles regarding the in situ efficacy of WRD devices were included into the



review. A flowchart of the article selection process is presented in Fig. 1.

General findings

There was a large variation between the included studies in methodology, reported outcome measures, preparation of the patient room prior to environmental sampling, the location of sampling within the room and the moment of sampling. This means that the findings were sometimes difficult to summarize. However, when the direction or magnitude of the effect was similar, outcomes have been combined when possible.

In articles reporting environmental outcome measures, the sites that were sampled within a room also differed per study and varied from high-touch surfaces to other specific surfaces within a patient room such as medical equipment or furniture. Moreover, the preparation prior to sampling differs between studies. In most studies the patient room was cleaned before disinfection, however some studies implemented WRD systems in an uncleaned room. The reported timing of sampling also varied from sampling before cleaning and after disinfection to sampling after cleaning and after disinfection to a combination of this.

Studies regarding clinical outcomes also varied in the reported outcome measures. The majority of the

included articles reported the microbial colonization (or acquired) infection rate (n = 14). Others reported the clinical infection rate (n = 4) or did not specify the infection rate (n = 1).

Additional file 1: Tables S1, S2, S3, S4, S5, S6, S7 and S8 show a complete overview of the included articles and their main outcomes .

Aerosolized hydrogen peroxide

Features

Aerosolized hydrogen peroxide (aHP) is a type of WRD in which a solution of 5–6% hydrogen peroxide is fogged into a patient room. During this process of fogging, a so-called ‘dry mist’ is formed which spreads through patient room and disinfects the contact surfaces [11]. Following exposure, hydrogen peroxide (HP) is naturally broken down to water and oxygen.

Practicalities

Automated room disinfection with aerosolized hydrogen peroxide has several benefits and limitations affecting the in situ efficacy. A benefit of aHP is that it is user friendly. The machine consists of only one unit and is therefore easy to transport within a hospital. Preparations of the patient room include cleaning and enlarging of the contact area. Although manufacturers state that the sealing

Table 2 In vitro efficacy of aHP for the preselected set of micro-organisms, expressed in log-reduction

| | Micro-organism | Effect in log ₁₀ reduction, median (range) | N (ref) |
|----------|----------------------|---|--------------------|
| Viruses | Norovirus | 2.5 (0.5–2.7) | 3 [12, 18, 19] |
| | (Surrogate) | 4.5 (>4–5.3) | 3 [18–20] |
| Bacteria | <i>Acinetobacter</i> | 2 (1–>4) | 2 [12, 16] |
| | CPE | | |
| | VRE | 1–1.7 | 1 [21] |
| | ESBL | >6 | 1 [14] |
| | MRSA | >4 (2–>6) | 4 [12, 14, 16, 17] |
| Spores | <i>C. difficile</i> | 4.9 (0.13–>5) | 4 [12, 14, 22, 23] |
| Yeast | <i>C. auris</i> | | |

sometimes the recommended ppm’s are not achieved rendering the performed procedure less or not effective. Similar to all other WRD devices, the efficacy of hydrogen peroxide is limited when a micro-organism is dissolved in (organic) material. Therefore, rooms must be cleaned (manually) before disinfection [12, 14, 15]. Compatibility of aHP with hospital materials has not been investigated thoroughly, but aHP seems compatible with metals, plastics and other materials.

In vitro efficacy

Ten articles have been included to assess the in vitro efficacy of aHP regarding the preselected micro-organisms (Table 2) [12, 14, 16–23]. For norovirus, the estimated reduction is 2.5-log for the virus itself and 4.5-log for its surrogate (Table 2) [18–20]. The in vitro efficacy regard-

Table 3 An overview of the environmental and clinical outcomes of studies using aerosolized hydrogen peroxide

| Micro-organism | Environmental outcomes | | | Clinical outcomes | | | |
|----------------|--------------------------------|---|--------------------|--------------------------------|---|-------------------|--------|
| | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | |
| Viruses | Norovirus | | | | | | |
| Bacteria | <i>Acinetobacter</i> | 78–100% reduction | | | | 2 [24, 25] | |
| | ESBL | | | | | | |
| | CPE | | | | | | |
| | MRSA | 10–100% reduction | 23.8% reduction | 4 [17, 26–28] | 41.1% reduction | 41.1% reduction | 1 [28] |
| | VRE | 100% reduction | | 1 [26] | | | |
| Spores | <i>C. difficile</i> | 59.4–94% reduction | 87.5–91% reduction | | | 3 [15, 29, 30] | |
| Yeast | <i>C. auris</i> | | | | | | |

of vents and doors with tape is not necessary, sealing is recommended by literature to prevent leakage of HP, which makes the preparations more labour intensive [12]. Furthermore, aHP is capable of disinfecting difficult-to-reach areas, such as the inside of a drawer or the back of a closet. However, aerosolized hydrogen peroxide particles are affected by gravity and aHP devices often distribute HP only in one direction due to the unidirectional nozzle [11]. Consequently, the distribution of aerosolized hydrogen peroxide in a room is sometimes not homogeneous.

A limitation of aerosolized hydrogen peroxide is the duration of disinfection. Hydrogen peroxide is toxic and therefore no people are allowed in the room during disinfection. A room that is disinfected with hydrogen peroxide may be re-entered only if the concentration of hydrogen peroxide has declined to 1 parts per million (ppm). The so-called aeration phase, the time between the injection of hydrogen peroxide in a room and the moment the room can be re-entered, is the main reason for the lengthy cycle time. For a single patient room, the cycle time is approximately 2–3 h [13–16]. Moreover,

ing bacteria shows a large variation, with relatively low log-reductions of 1–1.7 for VRE and *Acinetobacter* respectively, and higher reductions for MRSA (>4-log) and ESBL (>6-log) [12, 14, 16, 17, 21]. *C. difficile* shows a reduction of ~5-log [12, 14, 22, 23]. No research has been performed regarding aHP efficacy for CPE or *C. auris*.

In situ efficacy

For the assessment of in situ efficacy of aHP, nine articles have been included [15, 17, 24–30].

Environmental outcomes Environmental outcomes were described for *Acinetobacter*, MRSA, VRE and *C. difficile* (Table 3). All studies except for two reported the number of positive sites as an outcome measure. All studies observed a reduction in microbial contamination after disinfecting with aHP. Statistical significance was reported in only three out of the nine articles [15, 28, 30]. For *Acinetobacter*, a statistically non-significant 78–100% reduction in bacterial load was observed in two studies

Table 4 In vitro efficacy of H₂O₂ vapour for the preselected set of micro-organisms, expressed in log-reduction

| | Micro-organism | Effect in log ₁₀ reduction, median (range) | N (ref) |
|----------|----------------------|---|--------------------------------|
| Viruses | NoV | >4 | 1 [18] |
| | (Surrogaat) | 4.4 (3–≥6) | 4 [33, 34, 42, 43] |
| Bacteria | <i>Acinetobacter</i> | >5 (>4–>6) | 5 [12, 14, 35, 44, 45] |
| | CPE | >6 | 2 [44, 45] |
| | VRE | >6 (>4–>6) | 3 [35, 44, 45] |
| | ESBL | | |
| | MRSA | >6 (3–>6) | 7 [12, 14, 35, 36, 44, 46, 47] |
| Spores | <i>C. difficile</i> | >6 (>5,7–>6) | 6 [12, 23, 31, 37, 44, 48] |
| Yeasts | <i>C. auris</i> | | |

[24, 25]. Efficacy of aHP against MRSA ranged from a 10–100% reduction [17, 26–28]. Only one study reported significance and observed a statistically significant reduction in MRSA load of 23.8% [28]. One study investigated the efficacy of aHP against VRE and observed a complete reduction in bacterial load [26]. This study did not report significance. Lastly, a 59.4–94% reduction was observed for *C. difficile* after exposure to aHP. This range specifies to a reduction of 87.5–91% when merely observing the statistically significant outcomes [15, 29, 30]. No in situ studies were performed regarding norovirus, CPE, ESBL, and *Candida auris*.

Clinical outcomes Clinical efficacy of aHP was assessed for one study only (Table 3). Herein, a 41.1% ($p < 0.001$) reduction in hospital MRSA infection rate was observed after implementation of aHP following manual cleaning [28]. There were no in situ studies reporting hospital infection rates for the other pathogens.

H₂O₂ vapour

Features

Systems using H₂O₂ vapour evaporate a 30–35% hydrogen peroxide solution into a (patient) room. The hydrogen peroxide is broken down to water and oxygen after exposure. This decomposition is often facilitated by a aeration unit which reduces the disinfection cycle time [11].

Practicalities

Similar to aHP, a benefit of H₂O₂ vapour is its ability to disinfect difficult-to-reach areas. Moreover, due to heat-generated evaporation of hydrogen peroxide and the presence of multiple nozzles on the devices, the H₂O₂ vapour is homogeneously distributed amongst the patient room [11].

H₂O₂ vapour systems often consist of multiple units and are less straightforward in use than aHP systems. Moreover, the preparations before disinfection are time-consuming and labour intensive. To prevent leakage of

hydrogen peroxide, vents and entry doors must be sealed off. Disinfection with H₂O₂ vapour is time consuming. No people may remain in the room during disinfection and the patient room may only be re-entered if the concentration of hydrogen peroxide has declined under the health and safety exposure limit of 1 ppm. Due to the active aeration unit, the cycle time (the disinfection cycle excluding preparations) is somewhat shorter than that of aHP and is estimated at 1.5–2 h for a single patient room [13, 31–41]. Although most materials in a patient room are compatible with hydrogen peroxide, some materials or objects (e.g. nylon) can be damaged.

In vitro efficacy

H₂O₂ vapour has been shown to effectively reduce norovirus in in vitro settings, in which log reductions of >4-log have been observed (Table 4) [18, 33, 34, 42, 43]. For bacteria, reductions of >5-log were observed for *Acinetobacter* and of >6-log for CPE, VRE and MRSA [12, 14, 35, 36, 44–47]. Similarly, >6-log reductions were also observed for *C. difficile* [12, 23, 31, 37, 44, 48]. No studies are performed regarding the in vitro efficacy of ESBL and *C. auris*.

In situ efficacy

The in situ efficacy of H₂O₂ vapour has been assessed in a total of 11 articles [4, 6, 39–41, 49–54].

Environmental outcomes Environmental outcomes were described for *Acinetobacter*, MRSA, VRE and *C. difficile* (Table 5) [4, 6, 41, 49–54]. Three studies reported only number of positive rooms as an outcome measure, the others reported number of positive sites. Statistical significance was reported in only three studies [6, 41, 54]. For *Acinetobacter*, a 73–100% reduction in microbial load was observed after disinfection [6, 49]. Only the study reporting a 73% reduction described statistical significance [6]. Six studies regarding MRSA observed a range of effect from an increase of 11.1% to a reduction in contamination

Table 5 An overview of the environmental and clinical outcomes of studies using hydrogen peroxide vapour

| | Micro-organism | Environmental outcomes | | | Clinical outcomes | | |
|----------|----------------------|----------------------------------|---|---------------------|--------------------------------|---|-------------------|
| | | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies |
| Viruses | Norovirus | | | | | | |
| Bacteria | <i>Acinetobacter</i> | 73–100% reduction | 73% reduction | 2 [6, 49] | | | |
| | CPE | | | | | | |
| | ESBL | | | | | | |
| | MRSA | 11.1% increase to 100% reduction | 98.1% reduction | 7 [4, 6, 41, 50–53] | 68% reduction | | 1 [41] |
| | VRE | 6.4–100% reduction | | 2 [41, 50] | 79.3% reduction | 79.3% reduction | 1 [41] |
| Spores | <i>C. difficile</i> | 100% reduction | 100% reduction | 2 [41, 54] | 37–63% reduction | 37–60% reduction | 4 [39–41, 54] |
| Yeast | <i>C. auris</i> | | | | | | |

of 100% [4, 6, 50–53]. Only two of these studies reported significance [6, 41], of which one described a statistically significant reduction of 98.1% in MRSA contamination [6]. For VRE, a non-statistically significant reduction in bacterial load ranging from 6.4 to 100% was observed [41, 50]. Lastly, two studies observing *C. difficile* both reported a complete reduction in bacterial load after disinfection with H₂O₂ vapour [41, 54]. One of these studies was statistically significant [54]. No in situ studies regarding environmental outcomes were performed for norovirus, CPE, ESBL and *C. auris*.

Clinical outcomes Clinical efficacy of H₂O₂ vapour was assessed in four studies for MRSA, VRE and *C. difficile* (Table 5) [39–41, 54]. All studies reported a decrease in incidence rate. A non-significant reduction in MRSA infection rate was observed of 68%. The infection rate of VRE reduced significantly by 79.3% in a study by Passaretti et al. [41]. The range of effect of all studies for *C. difficile* was a reduction of 37–63%. The statistical range of effect was approximately similar with a 37–60% reduction. No studies regarding the infection rate were performed for norovirus, *Acinetobacter*, CPE, ESBL and *C. auris*.

Ultraviolet C

Features

Systems making use of ultraviolet C (UV-C) emit a radiation with a wavelength of 254 nm. This radiation is constantly emitted during the disinfection cycle. This radiation disrupts the stability of nucleic acids, which is fatal for a cell due to consequences on metabolism and cell division [55, 56].

A broad range of UV-C systems are currently offered on the market. A distinction can be made between

stationary systems and moving systems. Stationary systems have to be moved within the patient rooms by an operator in-between disinfection cycles to disinfect all areas. On the contrary, more advanced systems move autonomously through a patient room.

Practicalities

Automated room disinfection with ultraviolet radiation has several benefits and limitation. A benefit of disinfection with UV-C is the short disinfection time. In contrast with hydrogen peroxide, a room is immediately accessible after disinfection is complete as no aeration is needed. Disinfection of a single patient room with a stationary device is estimated at 50 min, while a moving robot takes 10–20 min [57, 58]. The room must be emptied of people during decontamination as exposure to UV radiation is not safe for humans. Moreover, UV-C disinfection does not make use of chemical products and leaves no residue rendering the process more environmental friendly [59].

A limitation of UV-C is that the efficacy of disinfection is reduced in areas that are out of the direct line of sight. UV-C is most effective when a micro-organism is directly exposed to the radiation. If a micro-organism is shaded from direct UV radiation, e.g. due to an obstruction or its inaccessible location, efficacy is limited [59]. Moreover, UV-C efficacy is reduced when the distance to an object that is to be disinfected increases or when the exposure time is limited [57, 60, 61]. To conclude, objects in a patient room containing polymers (i.e. medical devices and consumables) are susceptible to UV radiation and might be damaged by this type of WRD system.

Table 6 In vitro efficacy of UV-C for a preselected set of micro-organisms under optimal and suboptimal circumstances

| | Micro-organism | Optimal circumstances; effect in log ₁₀ reduction, median (range) | Suboptimal circumstances; effect in log ₁₀ reduction, median (range) | N (ref) |
|----------|----------------------|--|---|----------------------------|
| Viruses | Norovirus | | | |
| Bacteria | <i>Acinetobacter</i> | ≥ 4 (≥ 4→8) | 3 (< 1–4) | 6 [58, 61–65] |
| | CPE | 4–5 | 1–5 | 1 [66] |
| | ESBL | > 8 | > 3 | 2 [62, 65] |
| | MRSA | 4 (2–9) | < 3 (< 1→6) | 13 [58, 60–63, 65–72] |
| | VRE | 3.9 (2→8) | < 3 (< 1→4) | 10 [58, 60–63, 67–71] |
| Spores | <i>C. difficile</i> | 2.5 (1→5) | < 2 (0→3) | 11 [31, 57, 60, 61, 66–72] |
| Yeasts | <i>C. auris</i> | > 5 (3.99→6) | 3.3 (< 2→4) | 4 [72–75] |

Table 7 An overview of the environmental and clinical outcomes of studies using UV-C

| Micro-organism | Environmental outcomes | | | Clinical outcomes | | | |
|----------------|--------------------------------|---|-------------------------------|--------------------------------|---|----------------------|-------------------|
| | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | |
| Viruses | Norovirus | | | | | | |
| Bacteria | <i>Acinetobacter</i> | 35.8–98% reduction | 98% reduction | 2 [76, 77] | 53.1–71.8% reduction | 53.1–71.8% reduction | 3 [81–83] |
| | CPE | | | | 7.5% increase to 100% reduction | 100% reduction | 2 [82, 83] |
| | ESBL | | | | 12.9% reduction | | 1 [82] |
| | MRSA | 66.7–100% reduction | 79–97.5% reduction | 6 [60–62, 77–79] | 9.5% increase to 30.8% reduction | 30.8% reduction | 3 [81–83] |
| | VRE | 21.8–100% reduction | 83.3–100% reduction | 6 [60–62, 76–78] | 0.3–33.8% reduction | 0.3–33.8% reduction | 3 [81–83] |
| Spores | <i>C. difficile</i> | 23.9–100% reduction | 80–100% reduction | 6 [60, 76–80] | 26.1 increase to 46.2% reduction | 9.6–46.2% reduction | 5 [80, 81, 83–85] |
| Yeast | <i>C. auris</i> | 100% reduction after cleaning | 100% reduction after cleaning | 1 [79] | | | |

In vitro efficacy

UV-C elicits log reductions of ≥ 4 for all predefined bacteria under optimal conditions (Table 6) [58, 60–72]. ESBL is the most susceptible, where log reductions of > 8 have been shown [62, 65]. In vitro efficacy under suboptimal conditions is greatly reduced, with most bacteria showing reductions of approximately 3-log. For *C. difficile*, a reduction of 2.5-log is observed under optimal, and a < 2 -log reduction under suboptimal circumstances [31, 57, 60, 61, 66–72]. For *C. auris*, the optimal log reduction is > 5 and the suboptimal 3.3-log [72–75]. No studies were performed regarding norovirus.

Under suboptimal circumstances, the investigated micro-organism is diluted in organic soil, the sample does not receive direct UV-C light, received UV-C radiation for only a limited time or is placed at a further distance from the device. The in vitro efficacy is expressed in log reduction.

In situ efficacy

A total of 13 articles was published regarding the in situ efficacy of UV-C, of which 8 focused on environmental outcomes [60–62, 76–80] and 5 on clinical outcomes [81–85].

Environmental outcomes Two studies reported CFU as the outcome measure, one study reported the number of positive rooms and five studies reported the number of positive sites. All articles concerning the environmental outcomes reported a reduction in microbial contamination after disinfection (Table 7). For *Acinetobacter*, a total reduction of 35.8–98% in microbial load was observed [76, 77]. The reduction of 98% was statistically significant [77]. For MRSA, the range of effect of all studies ranged between a reduction of 66.7–100% and the statistically significant range between a 79–97.5% reduction [60–62, 77–79]. For VRE, a reduction of 21.8–100% in microbial contamination was reported [60–62, 76–78] the statis-

Table 8 In vitro efficacy of PX-UV for a preselected set of micro-organisms, expressed in log₁₀ reduction

| | Micro-organism | Optimal circumstances; effect in log ₁₀ reduction, median (range) | Suboptimal circumstances; effect in log ₁₀ reduction, median (range) | N (ref) |
|----------|----------------------|--|---|----------------|
| Viruses | Norovirus | | | |
| Bacteria | <i>Acinetobacter</i> | > 5 | | 1 [88] |
| | CPE | | | |
| | ESBL | > 5 | | 1 [88] |
| | MRSA | 3.3 (<2->5) | 1.5 (0.7-1.9) | 3 [68, 69, 88] |
| | VRE | 2.7 (<2->5) | 0.1-0.6 | 3 [68, 69, 88] |
| Spores | <i>C. difficile</i> | 1.8 (<1-3,4) | 0.7 (0.2-0.8) | 3 [68, 69, 88] |
| Yeasts | <i>C. auris</i> | 0.04-1.19 | | 2 [98, 99] |

tically significant range was considerably smaller with a 83.3–100% reduction. The range of effect of all studies associated with *C. difficile* ranged from a 23.9–100% reduction [60, 76–80]. The statistically significant range of effect was ranged between an 80–100% reduction. Only one study was performed regarding *C. auris* [79]. However, all *C. auris* had already been removed after the initial cleaning step, rendering additional disinfection unnecessary. No studies regarding the environmental decontamination were performed for norovirus, CPE and ESBL.

Clinical outcomes Large discrepancies between micro-organisms were observed in the assessment of clinical outcomes related to disinfection with UV-C (Table 7). The ranges of effect of all studies observed both increases and decreases in infection rate, whilst the statistically significant ranges of effect only reported decreases. For *Acinetobacter* and VRE, the total ranges of effect were similar to the significant ones and described respectively a 53.1–71.8% and a 0.3–33.8% reduction in infection rates. For CPE, the range of effect of all studies ran from a 7.5% increase to a 100% decrease [82, 83]. Only the study reporting a 100% decrease in infection rate was found statistically significant [82]. One study only reported the change in infection rate of ESBL after UV-C disinfection, which showed a non-significant 12.9% reduction [82]. Lastly, the range of effect of all studies for *C. difficile* ran from a 26.1% increase to a 46.2% decrease [80, 81, 83–85]. The statistically significant range only showed reductions in infection rate ranging between 9.6 and 46.2%. No studies regarding the infection rate were performed for norovirus and *C. auris*.

Pulsed-xenon UV

Features

Pulsed xenon ultraviolet (PX-UV) also make use of ultraviolet radiation. As opposed to UV-C, which only emits radiation at a constant wavelength, PX-UV emits radiation of a broad spectrum of wavelengths (200–320 nm).

This spectrum includes both UV-C, UV-B and UV-A radiation. Moreover, the radiation is not emitted continuously, but with short pulses [69, 86, 87].

Practicalities

The benefits and limitations of PX-UV are similar to those of UV-C devices. Disinfection of a single patient room with PX-UV, including the manual repositioning of the stationary device, only takes approximately 12–20 min [88–97]. Moreover, PX-UV devices are environmental friendly as no chemicals are used in the disinfection process and no residue is left.

Similar to UV-C, the main limitation of PX-UV is the limitation of its efficacy due to shading [68, 69, 88]. Other factors limiting the efficacy of UV are an increased distance between the device and the surface and a shortened disinfection time [69, 88, 98]. Moreover, as the device is stationary, it has to be repositioned by an operator during the disinfection cycle.

In vitro efficacy

There is considerable variety in efficacy of PX-UV between the predefined micro-organisms (Table 8). *Acinetobacter* and ESBL-producing bacteria are very susceptible to PX-UV, log reductions of > 5 have been observed under optimal circumstances [88]. On the contrary, MRSA and VRE show reduced susceptibility to PX-UV. Log reductions of 3.3 for MRSA and 2.7 for VRE have been reported previously under optimal circumstances [68, 69, 88]. Susceptibility is even further reduced when assessing efficacy under suboptimal circumstances. The reported log reductions were approximately two-fold lower for MRSA (1.5-log) and four-fold lower for VRE (0.1–0.6-log). *C. difficile* shows a log reduction of 1.8 under optimal conditions, and 0.7 under suboptimal circumstances [68, 69, 88]. The in vitro log reduction for *C. auris* is solely investigated under optimal circumstances, being 0.04–1.19-log [68,

Table 9 An overview of the environmental and clinical outcomes of studies using PX-UV

| Micro-organism | Environmental outcomes | | | Clinical outcomes | | | |
|----------------|--------------------------------|---|----------------------|--------------------------------|---|----------------------|---------------------------------|
| | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | Range of effect of all studies | Range of effect of stat. sign. findings | Number of studies | |
| Viruses | Norovirus | | | | | | |
| Bacteria | <i>Acinetobacter</i> | | | 63% reduction | 63% reduction | 1 [89] | |
| | CPE | | | | | | |
| | ESBL | | | | | | |
| | MRSA | 72.7–90.9% reduction | 72.7–90.9% reduction | 5 [69, 97, 100–102] | 20% increase to 37.9% reduction | 26.7–37.9% reduction | 4 [89, 92, 95, 107] |
| | VRE | 38–100% reduction | 75–100% reduction | 4 [69, 91, 103, 104] | 18.9% increase to 52.7% | 18.9–50% reduction | 4 [90, 92, 93, 107] |
| Spores | <i>C. difficile</i> | 59–100% reduction | 63.6–94.8% reduction | 3 [69, 105, 106] | 18.6% increase to 53% reduction | 17.2–53% reduction | 8 [85, 90, 92–94, 96, 107, 108] |
| Yeast | <i>C. auris</i> | | | | | | |

[69, 88]. No data in vitro data was available for norovirus and CPE.

In situ efficacy

A total of 20 articles were published regarding the in situ efficacy of PX-UV, of which 10 focused on environmental outcomes and 10 on clinical outcomes.

Environmental outcomes In situ efficacy of PX-UV regarding environmental outcomes has only been investigated for three of the preselected micro-organisms, being MRSA, VRE and *C. difficile* (Table 9). Five articles reported CFU/colonies as the outcome measure, the rest reported number of positive sites. All of the included articles observed a reduction in microbial contamination after disinfection. For MRSA, both total and statistically significant effect ranged from a 72.7–90.9% reduction in microbial contamination [69, 97, 100–102]. The statistically significant range of effect for VRE was considerably smaller than the total range of effect, respectively 38–100% reduction versus 75–100% reduction in contamination [69, 91, 103, 104]. For *C. difficile*, the total and statistically range of effect did not differ considerably, respectively 59–100% and 63.6–94.9% reduction in microbial contamination [69, 105, 106]. No studies were performed for norovirus, *Acinetobacter*, CPE, ESBL, and *C. auris*.

Clinical outcomes The ranges of effect of all studies for the preselected micro-organisms observed both increases and decreases in infection rate, whilst the statistically significant ranges of effect only reported decreases (Table 9). For *Acinetobacter*, a statistically significant reduction of 63% in infection rate was regarded [89]. For MRSA, the range of effect of all studies ran from a 20% increase in

infection rate to a 37.9% decrease [89, 92, 95, 107]. The statistically significant range only observed reductions in infection rate ranging from 26.7 to 37.9%. For VRE, that total range of effect ran from an increase of 18.9% to a decrease of 52.7%, while the statistically significant range ran from a 18.9% reduction to a 50% reduction [90, 92, 93, 107]. Lastly, the total *C. difficile* range also observed both increases and decreases in infection rate [85, 90, 92–94, 96, 107, 108]. The statistically significant range merely observed reductions ranging from 17.2 to 53%. No studies were performed for norovirus, CPE, ESBL and *C. auris*.

Comparison of WRD types

In the previous section of the results, we have presented the practical considerations, in vitro efficacy and in situ efficacy for the 4 typed of WRD devices. In Table 10, we show a side-by-side comparison of these data. The comparison must be regarded subjectively, as the outcomes do not stem from one article or source. More detailed information concerning the characteristics of the WRD devices can be found in the previous result sections.

Discussion

In this review, we summarized available literature about the in situ efficacy of four types of whole room disinfection devices, aerosolized hydrogen peroxide, H₂O₂ vapour, ultraviolet C and pulsed xenon ultraviolet, and assessed the differences with in vitro efficacy. In situ efficacy was determined by assessing environmental and clinical outcomes of the decontamination methods. The available literature was consistent in the observation that automated disinfection by any of the four WRD devices

Table 10 Comparison of the characteristics of aHP, H₂O₂ vapour, UV-C and PX-UV devices

| | aHP | H ₂ O ₂ vapour | UV-C | PX-UV |
|------------------------------------|---|---|--|---|
| In vitro efficacy | Viruses: 2.5-log Bacteria: >1 - >6-log Spores 4.9-log Fungi: – | Viruses: >4-log Bacteria: >5 - >6-log Spores >6-log Fungi: – | Viruses: – Bacteria: >3.9 - >8-log Spores 2.5-log Fungi: >5-log | Viruses: – Bacteria: >2.7 - >5-log Spores 1.8-log Fungi: 1-log |
| In situ efficacy | Reduction of environmental and clinical outcomes | Reduction of environmental and clinical outcomes | Reduction of environmental and clinical outcomes | Reduction of environmental and clinical outcomes |
| Homogeneity of disinfection | Not homogenous, unidirectional | Homogenous | Not homogenous under suboptimal circumstances | Not homogenous under suboptimal circumstances |
| Prior preparations in patient room | Cleaning, turning off smoke alarms | Cleaning, sealing doors/vents, turning off smoke alarms | Cleaning, removing curtains | Cleaning, removing curtains |
| Duration disinfection | 2–3 h | 1.5–2 h | Moving robot: 10–20 min Stationary robot: 50 min | 12–20 min |
| Required equipment | Device + disinfecting substance | Device + disinfecting substance | Device only | Device only |
| Compatibility materials | Not extensively investigated | Compatible with most materials | Might damage polymers | Not extensively investigated |

reduced the environmental and the clinical outcomes considerably. All WRD types were effective against various micro-organisms, reducing both environmental microbial contamination of patient rooms and infection rates among patients occupying those rooms.

No distinct variation or classification in in situ effectiveness of the WRD systems can be made, which contrasts to in vitro efficacy. When subjectively comparing the in vitro efficacies, H₂O₂ vapour achieves the highest microbial reduction of the four WRD types. This observation is also described in several other reviews and comparative studies [1, 12, 13, 31]. The in situ efficacy of the four WRD systems as described by the (significant) ranges of effect of environmental and clinical outcomes did not considerably vary between systems. Moreover, due to the variability in the included methodologies of included articles and the variability in the available information for specific WRD types and micro-organisms, firm conclusions regarding the differences of in situ efficacy of the four systems may not be drawn. The observation that all WRD systems lead to a reduction in both environmental outcomes as clinical outcomes is coherent with those made in other reviews [109–112].

Automated whole room disinfection systems did not completely remove the pathogens from the environment in all of the included studies, but did lead to a considerable decrease in the microbial load. Although a complete reduction of microbial contamination would be the most ideal scenario, this considerable decrease already lowers the chance of infection tremendously. Moreover, as a contrast to manual cleaning, the observed reduction in pathogens in a hospital setting is a constant and reliable outcome as it is not dependable of an operator. For

manual cleaning and disinfection, the decrease in microbial load is greatly dependent on the individual performing the procedure and is limited by human errors [1–3].

Considerations for choosing a WRD system

Due to the comparable in situ efficacy of the WRD systems, the assessment of what WRD device is most suitable in a specific healthcare setting may be mostly dependable on practical considerations. These considerations include among else the duration of disinfection, the preparations prior to disinfection, the purchase and operating costs, and the user friendliness of a device.

Even though WRD systems offer an unique opportunity for improved cleaning and disinfection practices, it is important to note that automated disinfection will never reduce the total time needed for the terminal cleaning and disinfection process as it always has to be preceded by (manual) cleaning. The added value of automated WRD lies in the enhancement of the quality of the terminal cleaning and disinfection process. In general, methods making use of UV are faster than methods making use of HP. After disinfection using UV, rooms are directly accessible. On the contrary, when disinfecting with HP, the concentration of HP first has to lower to 1 ppm before a room can be entered safely. Moreover, HP systems also require more preparations prior to disinfection which is labour intensive and time consuming. To prevent leakage of hydrogen peroxide, the rooms need to be sealed off from the external environment by shutting the doors with tape and covering the ventilation system. For UV, the main preparation is to enlarge the contact area and to decrease the shading area as much as possible. As

a consequence, HP-based WRD systems may be less suitable for the standard disinfection in healthcare settings that have a high patient turnover, due to the greater duration of disinfection and preparations.

In contrast to UV systems, HP systems are able to disinfect difficult-to-reach areas whilst UV-C systems are limited to exposed surfaces that are reached by UV radiation. H₂O₂ vapour systems are superior to aHP systems in this matter as they reach a more homogenous distribution of HP. The applicability of a system may therefore also be determined by the need or urgency to disinfect every inch of a patient room thoroughly. This may for example be dependent on the pathogenicity of microorganisms or its transmission route.

Regarding costs, devices making use of HP are less expensive in purchase than devices making use of UV radiation. However, user or operation costs are more expensive for HP devices as hydrogen peroxide tanks have to be replaced periodically whilst UV lamps only need changing once every few years; although the frequency depends on the intensity of usage.

To summarize, the choice for the most suitable WRD device cannot be summarized in a one-size-fits-all approach as the most suitable option relates to hospital-specific requirements.

Importance of manual cleaning

Automated room disinfection must always be preceded by a (manual) cleaning process. Both in vitro and in situ findings report that the effectiveness of WRD systems is limited in the presence of organic soil, such as blood or faeces [12, 15, 18, 29, 44, 57, 60, 88, 98]. Controversially, some in situ studies included in this review observed that also without cleaning, automated WRD (significantly) reduced microbial contamination [17, 25, 60–62, 69, 100]. However, as these studies were executed in a real-life hospital setting, it is expected that the rooms were not extremely soiled. They therefore do not invalidate the importance of cleaning before automated disinfection.

Importance of improved cleaning and disinfection

The importance of an improved cleaning and disinfection process, of which the replacement of manual disinfection by automated disinfection is an example, is highlighted by the current problem with antimicrobial resistance. The world health organization (WHO) has declared that antimicrobial resistance is one of the ten most pressing public health threats. The WHO stated that one of the factors contributing to the spread of microbes, of which some resistant to antimicrobial treatment, is inadequate infection prevention [113]. By improving microbial decontamination and therefore limiting the spread of micro-organisms, WRD could contribute

to the constraint of antimicrobial resistance. This effect could possibly be extra pronounced when the devices are implemented in countries with high antimicrobial resistance (in which implementation is feasible). A study researching antibiotic resistance in 41 countries identified that low and middle income countries show higher antimicrobial rates than high-income countries with the drug resistance index being in India [114]. Within Europe, the most recent data as published by the European Centre for Disease Prevention and Control (ECDC) in 2019 observed that most resistant isolates were detected in Greece, Romania, Italy and Bulgaria [115].

Strength and limitations

A main strength of this review is its systematic approach in reviewing literature. Moreover, it is presumed that this review is the first to give a simultaneous overview of both in situ and in vitro efficacy, as well as practical considerations of the WRD systems. Moreover, besides reporting solely the environmental outcomes, this review also gave insight into the effect of WRD systems on both environmental and clinical outcomes.

The main limitation of this review is the substantial variation in methodology and outcome measures of the included studies. Moreover, the availability of data was also limited to only a section of the preselected microorganisms. As a consequence, no specific conclusions can be made regarding the in situ efficacy of the WRD devices. Nonetheless, a general conclusion that can be drawn is that all WRD systems are effective in reducing the pathogenic load in a hospital setting. Another limitation of this review is that no distinction was made in the clinical outcome measure between microbial colonization (acquisition) infection rates and clinical infection rates. Stratification could not be performed as this would lead to a too limited number of articles. A final limitation of this review is that most included studies are performed in a high-income or resource countries. As the infection rates greatly vary between high and middle-to-low income countries, the results of this review might not directly relate to low or middle income countries.

Recommendations

Due to the variability in research methodologies of the included articles, this review can only generally conclude that all WRD systems are effective in a healthcare setting. It is however not possible to conclude what system is most effective in situ. As such data could influence the choice for the best fitting WRD device in a specific healthcare setting, we recommend the initiation of a study that directly compares the four types of WRD devices regarding their in situ efficacy. If such a study uses a standardized protocol assessing preferably

both environmental and clinical outcome measures for all WRD devices and for a range of pathogens, it would be possible to compare the in situ efficacy of the different types of WRD devices. Moreover, we recommend to base the choice for the best fitting automated WRD device in a healthcare setting as much on other practical considerations, such as disinfection time and preparation of a patient room, as on efficacy or even more. These practical considerations will eventually determine how well a device performs with a healthcare setting.

Conclusion

In conclusion, despite the large variation in the included studies, all automated WRD systems (aHP, H₂O₂ vapour, UV-C and PX-UV) are effective in reducing the amount of pathogens present in a hospital environment. Due to the comparable in situ effectiveness of the WRD systems, the assessment of what WRD device is most suitable in a specific healthcare setting may mostly depend on practical considerations.

Abbreviations

A. baumannii: *Acinetobacter baumannii*; aHP: Aerosolized hydrogen peroxide; whole room disinfection system making use of a 5–6% hydrogen peroxide solution; *C. auris*: *Candida auris*; *C. difficile*: *Clostridium difficile*; CPE: Carbapenemase-producing enterobacteriaceae; CFU: Colony-forming units; ESBL: Extended spectrum beta-lactamase; HAI: Hospital-acquired infection; H₂O₂ vapour: Whole room disinfection system making use of a 30–35% hydrogen peroxide solution; HP: Hydrogen peroxide; HPV: A type of H₂O₂ vapour device produced by the manufacturer Bioquell; MDRO: Multidrug resistant micro-organism; MRSA: Methicillin-resistant *Staphylococcus aureus*; NoV: Norovirus; PX-UV: Pulsed xenon ultraviolet; whole room disinfection system making use of pulsing UV radiation; UV: Ultraviolet; UV-C: Ultraviolet C; whole room disinfection making use of UV radiation within the UV-C spectrum; VRE: Vancomycin-resistant enterococcus; WRD: Whole room disinfection.

Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s13756-022-01183-y>.

Additional file 1: Table S1. The in situ efficacy of aerosolized hydrogen peroxide (aHP) as expressed in environmental outcomes. **Table S2.** The in situ efficacy of aerosolized hydrogen peroxide (aHP) as expressed in clinical outcomes. **Table S3.** The in situ efficacy of H₂O₂ vapour as expressed in environmental outcomes. **Table S4.** The in situ efficacy of H₂O₂ vapour as expressed in clinical outcomes. **Table S5.** The in situ efficacy of ultraviolet C (UV-C) as expressed in environmental outcomes. **Table S6.** The in situ efficacy of ultraviolet C (UV-C) as expressed in clinical outcomes. **Table S7.** The in situ efficacy of pulsed xenon ultraviolet (PX-UV) as expressed in environmental outcomes. **Table S8.** The in situ efficacy of pulsed xenon ultraviolet (PX-UV) as expressed in clinical outcomes.

Acknowledgements

Not applicable.

Author contributions

CS collected and processed the literature used in this review and was responsible for the development of the manuscript. AT was the main supervisor, contributed to the methodology and content of the paper. SC and EB provided

supervision concerning the content of the paper, especially in the subject of infection prevention and control. CR critically assessed the article selection and selection methodology. All authors contributed to the reviewing and editing of the final manuscript.

Funding

Not applicable.

Availability of data and materials

The articles included in this literature review were all retrieved from PubMed and can be found in the citations.

Declarations

Ethics approval and consent to participate

Not applicable.

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

Received: 15 July 2022 Accepted: 10 November 2022

Published online: 05 December 2022

References

- Otter JA, Yezli S, Barbut F, Perl TM. An overview of automated room disinfection systems: when to use them and how to choose them. In: Walker J, editor. Decontamination in Hospitals and Healthcare. 2nd Ed. Woodhead Publishing Series in Biomaterials. Woodhead Publishing; 2020. p. 323–69.
- Fraise A. Currently available sporicides for use in healthcare, and their limitations. *J Hosp Infect.* 2011;77(3):210–2.
- Carling PC, Parry MM, Rupp ME, Po JL, Dick B, Von Behren S, et al. Improving cleaning of the environment surrounding patients in 36 acute care hospitals. *Infect Control Hosp Epidemiol.* 2008;29(11):1035–41.
- French GL, Otter JA, Shannon K, Adams N, Watling D, Parks M. Tackling contamination of the hospital environment by methicillin-resistant *Staphylococcus aureus* (MRSA): a comparison between conventional terminal cleaning and hydrogen peroxide vapour decontamination. *J Hosp Infect.* 2004;57(1):31–7.
- Byers KE, Durbin LJ, Simonton BM, Anglim AM, Adal KA, Farr BM. Disinfection of hospital rooms contaminated with vancomycin-resistant enterococci. *Infect Control Hosp Epidemiol.* 1998;19(4):261–4.
- Manian FA, Griesenauer S, Senkel D, Setzer JM, Doll SA, Perry AM, et al. Isolation of *Acinetobacter baumannii* complex and methicillin-resistant *Staphylococcus aureus* from hospital rooms following terminal cleaning and disinfection: can we do better? *Infect Control Hosp Epidemiol.* 2011;32(7):667–72.
- Wilcox M, Fawley W, Wigglesworth N, Parnell P, Verity P, Freeman J. Comparison of the effect of detergent versus hypochlorite cleaning on environmental contamination and incidence of *Clostridium difficile* infection. *J Hosp Infect.* 2003;54(2):109–14.
- Huang SS, Datta R, Platt R. Risk of acquiring antibiotic-resistant bacteria from prior room occupants. *Arch Intern Med.* 2006;166(18):1945–51.
- Drees M, Snyderman DR, Schmid CH, Barefoot L, Hansjosten K, Vue PM, et al. Prior environmental contamination increases the risk of acquisition of vancomycin-resistant enterococci. *Clin Infect Dis.* 2008;46(5):678–85.
- Nseir S, Blazejewski C, Lubret R, Wallet F, Courcol R, Durocher A. Risk of acquiring multidrug-resistant Gram-negative bacilli from prior room occupants in the intensive care unit. *Clin Microbiol Infect.* 2011;17(8):1201–8.
- Otter JA, Yezli S, Barbut F, Perl TM. 15 - an overview of automated room disinfection systems: when to use them and how to choose them. In:

- Walker J, editor. Decontamination in hospitals and healthcare. Second Edition); Woodhead Publishing; 2020. p. 323–69.
12. Fu T, Gent P, Kumar V. Efficacy, efficiency and safety aspects of hydrogen peroxide vapour and aerosolized hydrogen peroxide room disinfection systems. *J Hosp Infect.* 2012;80(3):199–205.
 13. Holmdahl T, Lanbeck P, Wullt M, Walder MH. A head-to-head comparison of hydrogen peroxide vapor and aerosol room decontamination systems. *Infect Control Hosp Epidemiol.* 2011;32(9):831–6.
 14. Ali S, Muzslay M, Bruce M, Jeanes A, Moore G, Wilson A. Efficacy of two hydrogen peroxide vapour aerial decontamination systems for enhanced disinfection of methicillin-resistant *Staphylococcus aureus*, *Klebsiella pneumoniae* and *Clostridium difficile* in single isolation rooms. *J Hosp Infect.* 2016;93(1):70–7.
 15. Shapey S, Machin K, Levi K, Boswell TC. Activity of a dry mist hydrogen peroxide system against environmental *Clostridium difficile* contamination in elderly care wards. *J Hosp Infect.* 2008;70(2):136–41.
 16. Piskin N, Celebi G, Kulah C, Mengelolu Z, Yumusak M. Activity of a dry mist-generated hydrogen peroxide disinfection system against methicillin-resistant *Staphylococcus aureus* and *Acinetobacter baumannii*. *Am J Infect Control.* 2011;39(9):757–62.
 17. Bartels M, Kristoffersen K, Slotsbjerg T, Rohde S, Lundgren B, Westh H. Environmental methicillin-resistant *Staphylococcus aureus* (MRSA) disinfection using dry-mist-generated hydrogen peroxide. *J Hosp Infect.* 2008;70(1):35–41.
 18. Tuladhar E, Terpstra P, Koopmans M, Duizer E. Virucidal efficacy of hydrogen peroxide vapour disinfection. *J Hosp Infect.* 2012;80(2):110–5.
 19. Montazeri N, Manuel C, Moorman E, Khatiwada JR, Williams LL, Jaykus L-A. Virucidal activity of fogged chlorine dioxide-and hydrogen peroxide-based disinfectants against human norovirus and its surrogate, feline calicivirus, on hard-to-reach surfaces. *Front Microbiol.* 2017;8:1031.
 20. Zonta W, Mauroy A, Farnir F, Thiry E. Virucidal efficacy of a hydrogen peroxide nebulization against murine norovirus and feline calicivirus, two surrogates of human norovirus. *Food Environ Virol.* 2016;8(4):275–82.
 21. Chan HT, White P, Sheorey H, Cocks J, Waters MJ. Evaluation of the biological efficacy of hydrogen peroxide vapour decontamination in wards of an Australian hospital. *J Hosp Infect.* 2011;79(2):125–8.
 22. Steindl G, Fiedler A, Huhulescu S, Wewalka G, Allerberger F. Effect of airborne hydrogen peroxide on spores of *Clostridium difficile*. *Wien Klinische Wochenschr.* 2015;127(11):421–6.
 23. Beswick AJ, Farrant J, Makison C, Gawn J, Frost G, Crook B, et al. Comparison of multiple systems for laboratory whole room fumigation. *Appl Biosaf.* 2011;16(3):139–57.
 24. Coimbra L, Pinto Silva A, Pina-Vaz C, Rodrigues A. Effective disinfection of a burn unit after two cases of sepsis caused by multi-drug-resistant *Acinetobacter baumannii*. *Surg Infect (Larchmt).* 2018;19(5):541–3.
 25. Lerner AO, Abu-Hanna J, Carmeli Y, Schechner V. Environmental contamination by carbapenem-resistant *Acinetobacter baumannii*: the effects of room type and cleaning methods. *Infect Control Hosp Epidemiol.* 2020;41(2):166–71.
 26. McKew G, Phan T, Cai T, Taggart S, Cheong E, Gottlieb T. Efficacy of aerosolized hydrogen peroxide (Deprox) cleaning compared to physical cleaning in a Burns Unit. *Infect Dis Health.* 2021;26(3):161–5.
 27. Taneja N, Biswal M, Kumar A, Edwin A, Sunita T, Emmanuel R, et al. Hydrogen peroxide vapour for decontaminating air-conditioning ducts and rooms of an emergency complex in northern India: time to move on. *J Hosp Infect.* 2011;78(3):200–3.
 28. Mitchell BG, Digney W, Locket P, Dancer SJ. Controlling methicillin-resistant *Staphylococcus aureus* (MRSA) in a hospital and the role of hydrogen peroxide decontamination: an interrupted time series analysis. *Bmj Open.* 2014;4(4):e004522.
 29. Yui S, Ali S, Muzslay M, Jeanes A, Wilson APR. Identification of *Clostridium difficile* reservoirs in the patient environment and efficacy of aerial hydrogen peroxide decontamination. *Infect Control Hosp Epidemiol.* 2017;38(12):1487–92.
 30. Barbut F, Menuet D, Verachten M, Girou E. Comparison of the efficacy of a hydrogen peroxide dry-mist disinfection system and sodium hypochlorite solution for eradication of *Clostridium difficile* spores. *Infect Control Hosp Epidemiol.* 2009;30(6):507–14.
 31. Havill NL, Moore BA, Boyce JM. Comparison of the microbiological efficacy of hydrogen peroxide vapor and ultraviolet light processes for room decontamination. *Infect Control Hosp Epidemiol.* 2012;33(5):507–12.
 32. Blazejewski C, Wallet F, Rouzé A, Le Guern R, Ponthieux S, Salleron J, et al. Efficiency of hydrogen peroxide in improving disinfection of ICU rooms. *Crit Care.* 2015;19(1):30.
 33. Goyal SM, Chander Y, Yezli S, Otter J. Evaluating the virucidal efficacy of hydrogen peroxide vapour. *J Hosp Infect.* 2014;86(4):255–9.
 34. Holmdahl T, Walder M, Uzcátegui N, Odenholt J, Lanbeck P, Medstrand P, et al. Hydrogen peroxide vapor decontamination in a patient room using feline calicivirus and murine norovirus as surrogate markers for human norovirus. *Infect Control Hosp Epidemiol.* 2016;37(5):561–6.
 35. Lemmen S, Scheithauer S, Häfner H, Yezli S, Mohr M, Otter JA. Evaluation of hydrogen peroxide vapor for the inactivation of nosocomial pathogens on porous and nonporous surfaces. *Am J Infect Control.* 2015;43(1):82–5.
 36. Murdoch L, Bailey L, Banham E, Watson F, Adams N, Chewins J. Evaluating different concentrations of hydrogen peroxide in an automated room disinfection system. *Lett Appl Microbiol.* 2016;63(3):178–82.
 37. Barbut F, Yezli S, Otter J. Activity in vitro of hydrogen peroxide vapour against *Clostridium difficile* spores. *J Hosp Infect.* 2012;80(1):85–7.
 38. Chiguer M, Maleb A, Amrani R, Abda N, Alami Z. Assessment of surface cleaning and disinfection in neonatal intensive care unit. *Heliyon.* 2019;5(12):e02966.
 39. Manian FA, Griesnauer S, Bryant A. Implementation of hospital-wide enhanced terminal cleaning of targeted patient rooms and its impact on endemic *Clostridium difficile* infection rates. *Am J Infect Control.* 2013;41(6):537–41.
 40. McCord J, Prewitt M, Dyakova E, Mookerjee S, Otter JA. Reduction in *Clostridium difficile* infection associated with the introduction of hydrogen peroxide vapour automated room disinfection. *J Hosp Infect.* 2016;94(2):185–7.
 41. Passaretti CL, Otter JA, Reich NG, Myers J, Shepard J, Ross T, et al. An evaluation of environmental decontamination with hydrogen peroxide vapor for reducing the risk of patient acquisition of multidrug-resistant organisms. *Clin Infect Dis.* 2013;56(1):27–35.
 42. Bentley K, Dove B, Parks S, Walker J, Bennett A. Hydrogen peroxide vapour decontamination of surfaces artificially contaminated with norovirus surrogate feline calicivirus. *J Hosp Infect.* 2012;80(2):116–21.
 43. Goyal S, Chander Y, Yezli S, Otter J. P08. 02 Hydrogen peroxide vapor (HPV) inactivation of feline calicivirus, a surrogate for norovirus. *J Hosp Infect.* 2010;76:22–53.
 44. Otter JA, French GL. Survival of nosocomial bacteria and spores on surfaces and inactivation by hydrogen peroxide vapor. *J Clin Microbiol.* 2009;47(1):205–7.
 45. Watson F, Keevil C, Wilks S, Chewins J. Modelling vaporized hydrogen peroxide efficacy against mono-species biofilms. *Sci Rep.* 2018;8(1):1–7.
 46. Pottage T, Macken S, Walker J, Bennett A. Methicillin-resistant *Staphylococcus aureus* is more resistant to vaporized hydrogen peroxide than commercial *Geobacillus stearothermophilus* biological indicators. *J Hosp Infect.* 2012;80(1):41–5.
 47. Otter J, Yezli S, French G. Impact of the suspending medium on susceptibility of methicillin-resistant *Staphylococcus aureus* to hydrogen peroxide vapour decontamination. *J Hosp Infect.* 2012;82(3):213–5.
 48. Lawley TD, Clare S, Deakin LJ, Goulding D, Yen JL, Raisen C, et al. Use of purified *Clostridium difficile* spores to facilitate evaluation of health care disinfection regimens. *Appl Environ Microbiol.* 2010;76(20):6895–900.
 49. Otter JA, Yezli S, Schouten MA, van Zanten ARH, Houmes-Zielman G, Nohlmans-Paulssen MKE. Hydrogen peroxide vapor decontamination of an intensive care unit to remove environmental reservoirs of multidrug-resistant gram-negative rods during an outbreak. *Am J Infect Control.* 2010;38(9):754–6.
 50. Otter JA, Cummins M, Ahmad F, van Tonder C, Drabu YJ. Assessing the biological efficacy and rate of recontamination following hydrogen peroxide vapour decontamination. *J Hosp Infect.* 2007;67(2):182–8.
 51. Dryden M, Parnaby R, Dailly S, Lewis T, Davis-Blues K, Otter JA, et al. Hydrogen peroxide vapour decontamination in the control of a polyclonal methicillin-resistant *Staphylococcus aureus* outbreak on a surgical ward. *J Hosp Infect.* 2008;68(2):190–2.
 52. Jeanes A, Rao G, Osman M, Merrick P. Eradication of persistent environmental MRSA. *J Hosp Infect.* 2005;61(1):85–6.

53. Hardy KJ, Gossain S, Henderson N, Drugan C, Oppenheim BA, Gao F, et al. Rapid recontamination with MRSA of the environment of an intensive care unit after decontamination with hydrogen peroxide vapour. *J Hosp Infect.* 2007;66(4):360–8.
54. Boyce JM, Havill NL, Otter JA, McDonald LC, Adams NM, Cooper T, et al. Impact of hydrogen peroxide vapor room decontamination on *Clostridium difficile* environmental contamination and transmission in a healthcare setting. *Infect Control Hosp Epidemiol.* 2008;29(8):723–9.
55. Kowalski W. *Ultraviolet germicidal irradiation handbook: UVGI for air and surface disinfection.* Berlin, Heidelberg: Springer; 2010.
56. Cutler TD, Zimmerman JJ. Ultraviolet irradiation and the mechanisms underlying its inactivation of infectious agents. *Anim Health Res Reviews.* 2011;12(1):15–23.
57. Boyce JM, Havill NL, Moore BA. Terminal decontamination of patient rooms using an automated mobile UV light unit. *Infect Control Hosp Epidemiol.* 2011;32(8):737–42.
58. Mahida N, Vaughan N, Boswell T. First UK evaluation of an automated ultraviolet-C room decontamination device (Tru-D™). *J Hosp Infect.* 2013;84(4):332–5.
59. Diab-El Schahawi M, Zingg W, Vos M, Humphreys H, Lopez-Cerero L, Fueszl A, et al. Ultraviolet disinfection robots to improve hospital cleaning: Real promise or just a gimmick? *Antimicrob Resist Infect Control.* 2021;10(1):1–3.
60. Nerandzic MM, Cadnum JL, Pultz MJ, Donskey CJ. Evaluation of an automated ultraviolet radiation device for decontamination of *Clostridium difficile* and other healthcare-associated pathogens in hospital rooms. *BMC Infect Dis.* 2010;10:197.
61. Rutala WA, Gergen MF, Weber DJ. Room decontamination with UV radiation. *Infect Control Hosp Epidemiol.* 2010;31(10):1025–9.
62. Yang JH, Wu UI, Tai HM, Sheng WH. Effectiveness of an ultraviolet-C disinfection system for reduction of healthcare-associated pathogens. *J Microbiol Immunol Infect.* 2019;52(3):487–93.
63. Nottingham M, Peterson G, Doern C, Doll M, Masroor N, Sanogo K, et al. Ultraviolet-C light as a means of disinfecting anesthesia workstations. *Am J Infect Control.* 2017;45(9):1011–3.
64. Rastogi VK, Wallace L, Smith LS. Disinfection of *Acinetobacter baumannii*-contaminated surfaces relevant to medical treatment facilities with ultraviolet C light. *Mil Med.* 2007;172(11):1166–9.
65. Pholawat Tingpej M, Tiengtip R. Decontamination efficacy of ultraviolet radiation against biofilms of common nosocomial bacteria. *J Med Assoc Thai.* 2015;98(6):582–8.
66. Ali S, Yui S, Muzslay M, Wilson A. Comparison of two whole-room ultraviolet irradiation systems for enhanced disinfection of contaminated hospital patient rooms. *J Hosp Infect.* 2017;97(2):180–4.
67. Mitchell J, Sifuentes L, Wissler A, Abd-Elmaksoud S, Lopez G, Gerba CP. Modelling of ultraviolet light inactivation kinetics of methicillin-resistant *Staphylococcus aureus*, vancomycin-resistant *Enterococcus*, *Clostridium difficile* spores and murine norovirus on fomite surfaces. *J Appl Microbiol.* 2019;126(1):58–67.
68. Cadnum JL, Jencson AL, Gestrich SA, Livingston SH, Karaman BA, Benner KJ, et al. A comparison of the efficacy of multiple ultraviolet light room decontamination devices in a radiology procedure room. *Infect Control Hosp Epidemiol.* 2019;40(2):158–63.
69. Nerandzic MM, Thota P, Sankar CT, Jencson A, Cadnum JL, Ray AJ, et al. Evaluation of a pulsed xenon ultraviolet disinfection system for reduction of healthcare-associated pathogens in hospital rooms. *Infect Control Hosp Epidemiol.* 2015;36(2):192–7.
70. Nerandzic MM, Fisher CW, Donskey CJ. Sorting through the wealth of options: comparative evaluation of two ultraviolet disinfection systems. *PLoS ONE.* 2014;9(9):e107444.
71. Boyce JM, Farrel PA, Towle D, Fekietta R, Aniskiewicz M. Impact of room location on UV-C irradiance and UV-C dosage and antimicrobial effect delivered by a mobile UV-C light device. *Infect Control Hosp Epidemiol.* 2016;37(6):667–72.
72. Cadnum JL, Shaikh AA, Piedrahita CT, Jencson AL, Larkin EL, Ghannoum MA, et al. Relative resistance of the emerging fungal pathogen *Candida auris* and other *Candida* species to killing by ultraviolet light. *Infect Control Hosp Epidemiol.* 2018;39(1):94–6.
73. de Groot T, Chowdhary A, Meis JF, Voss A. Killing of *Candida auris* by UV-C: importance of exposure time and distance. *Mycoses.* 2019;62(5):408–12.
74. Fu L, Le T, Liu Z, Wang L, Guo H, Yang J, et al. Different efficacies of common disinfection methods against *Candida auris* and other *Candida* species. *J Infect Public Health.* 2020;13(5):730–6.
75. Ponnachan P, Vinod V, Pullanhi U, Varma P, Singh S, Biswas R, et al. Antifungal activity of octenidine dihydrochloride and ultraviolet-C light against multidrug-resistant *Candida auris*. *J Hosp Infect.* 2019;102(1):120–4.
76. Anderson DJ, Gergen MF, Smathers E, Sexton DJ, Chen LF, Weber DJ, et al. Decontamination of targeted pathogens from patient rooms using an automated ultraviolet-C-emitting device. *Infect Control Hosp Epidemiol.* 2013;34(5):466–71.
77. Rutala WA, Kanamori H, Gergen MF, Knelson LP, Sickbert-Bennett EE, Chen LF, et al. Enhanced disinfection leads to reduction of microbial contamination and a decrease in patient colonization and infection. *Infect Control Hosp Epidemiol.* 2018;39(9):1118–21.
78. Wong T, Woznow T, Petrie M, Murzello E, Muniak A, Kadora A, et al. Postdischarge decontamination of MRSA, VRE, and *Clostridium difficile* isolation rooms using 2 commercially available automated ultraviolet-C-emitting devices. *Am J Infect Control.* 2016;44(4):416–20.
79. Mustapha A, Alhmidhi H, Cadnum JL, Jencson AL, Donskey CJ. Efficacy of manual cleaning and an ultraviolet C room decontamination device in reducing health care-associated pathogens on hospital floors. *Am J Infect Control.* 2018;46(5):584–6.
80. Liscyenesky C, Hines LP, Smyer J, Hanrahan M, Orellana RC, Mangino JE. The effect of ultraviolet light on *Clostridium difficile* spore recovery versus bleach alone. *Infect Control Hosp Epidemiol.* 2017;38(9):1116–7.
81. Anderson DJ, Moehring RW, Weber DJ, Lewis SS, Chen LF, Schwab JC, et al. Effectiveness of targeted enhanced terminal room disinfection on hospital-wide acquisition and infection with multidrug-resistant organisms and *Clostridium difficile*: a secondary analysis of a multi-center cluster randomised controlled trial with crossover design (BETR Disinfection). *Lancet Infect Dis.* 2018;18(8):845–53.
82. Raggi R, Archulet K, Haag CW, Tang W. Clinical, operational, and financial impact of an ultraviolet-C terminal disinfection intervention at a community hospital. *Am J Infect Control.* 2018;46(11):1224–9.
83. Napolitano NA, Mahapatra T, Tang W. The effectiveness of UV-C radiation for facility-wide environmental disinfection to reduce health care-acquired infections. *Am J Infect Control.* 2015;43(12):1342–6.
84. Pegues DA, Han J, Gilmar C, McDonnell B, Gaynes S. Impact of ultraviolet germicidal irradiation for no-touch terminal room disinfection on *Clostridium difficile* infection incidence among hematology-oncology patients. *Infect Control Hosp Epidemiol.* 2017;38(1):39–44.
85. McMullen K, Guth RM, Wood H, Mueller C, Dunn G, Wade R, et al. Impact of no-touch ultraviolet light room disinfection systems on *Clostridioides difficile* infections. *Am J Infect Control.* 2021;49(5):646–8.
86. Casini B, Tuvo B, Cristina ML, Spagnolo AM, Totaro M, Baggiani A, et al. Evaluation of an ultraviolet C (UVC) light-emitting device for disinfection of high touch surfaces in hospital critical areas. *Int J Environ Res Public Health.* 2019;16:19.
87. Song L, Li W, He J, Li L, Li T, Gu D, Tang H. Development of a pulsed xenon ultraviolet disinfection device for real-time air disinfection in ambulances. *J Healthc Eng.* 2020;2020:6053065. <https://doi.org/10.1155/2020/6053065>.
88. Kitagawa H, Tadera K, Hara T, Kashiya S, Mori M, Ohge H. Efficacy of pulsed xenon ultraviolet disinfection of multidrug-resistant bacteria and *Clostridioides difficile* spores. *Infect Disease Health.* 2020;25(3):181–5.
89. Morikane K, Suzuki S, Yoshioka J, Yakuwa J, Nakane M, Nemoto K. Clinical and microbiological effect of pulsed xenon ultraviolet disinfection to reduce multidrug-resistant organisms in the intensive care unit in a Japanese hospital: a before-after study. *BMC Infect Dis.* 2020;20(1):82.
90. Brite J, McMillen T, Robilotti E, Sun J, Chow HY, Stell F, et al. Effectiveness of ultraviolet disinfection in reducing hospital-acquired *Clostridium difficile* and vancomycin-resistant *enterococcus* on a bone marrow transplant unit. *Infect Control Hosp Epidemiol.* 2018;39(11):1301–6.
91. Beal A, Mahida N, Staniforth K, Vaughan N, Clarke M, Boswell T. First UK trial of Xenex PX-UV, an automated ultraviolet room decontamination device in a clinical haematology and bone marrow transplantation unit. *J Hosp Infect.* 2016;93(2):164–8.

92. Vianna PG, Dale CR Jr, Simmons S, Stibich M, Licitra CM. Impact of pulsed xenon ultraviolet light on hospital-acquired infection rates in a community hospital. *Am J Infect Control*. 2016;44(3):299–303.
93. Sampathkumar P, Folkert C, Barth JE, Nation L, Benz M, Hesse A, et al. A trial of pulsed xenon ultraviolet disinfection to reduce *Clostridioides difficile* infection. *Am J Infect Control*. 2019;47(4):406–8.
94. Nagaraja A, Visintainer P, Haas JP, Menz J, Wormser GP, Montecalvo MA. *Clostridium difficile* infections before and during use of ultraviolet disinfection. *Am J Infect Control*. 2015;43(9):940–5.
95. Kitagawa H, Mori M, Kawano R, Hara T, Kashiyama S, Hayashi Y, et al. Combining pulsed xenon ultraviolet disinfection with terminal manual cleaning helps reduce the acquisition rate of methicillin-resistant *Staphylococcus aureus*. *Am J Infect Control*. 2021;49(8):1048–51.
96. Attia F, Whitener C, Mincemoyer S, Houck J, Julian K. The effect of pulsed xenon ultraviolet light disinfection on healthcare-associated *Clostridioides difficile* rates in a tertiary care hospital. *Am J Infect Control*. 2020;48(9):1116–8.
97. Zeber JE, Pfeiffer C, Baddley JW, Cadena-Zuluaga J, Stock EM, Copeland LA, et al. Effect of pulsed xenon ultraviolet room disinfection devices on microbial counts for methicillin-resistant *Staphylococcus aureus* and aerobic bacterial colonies. *Am J Infect Control*. 2018;46(6):668–73.
98. Maslo C, du Plooy M, Coetzee J. The efficacy of pulsed-xenon ultraviolet light technology on *Candida auris*. *BMC Infect Dis*. 2019;19(1):1–3.
99. Chatterjee P, Choi H, Ochoa B, Garmon G, Coppin JD, Allton Y, et al. Clade-specific variation in susceptibility of *Candida auris* to broad-spectrum ultraviolet C light (UV-C). *Infect Control Hosp Epidemiol*. 2020;41(12):1384–7.
100. Jinadatha C, Villamaria FC, Restrepo MI, Ganachari-Mallappa N, Liao IC, Stock EM, et al. Is the pulsed xenon ultraviolet light no-touch disinfection system effective on methicillin-resistant *Staphylococcus aureus* in the absence of manual cleaning? *Am J Infect Control*. 2015;43(8):878–81.
101. Jinadatha C, Quezada R, Huber TW, Williams JB, Zeber JE, Copeland LA. Evaluation of a pulsed-xenon ultraviolet room disinfection device for impact on contamination levels of methicillin-resistant *Staphylococcus aureus*. *BMC Infect Dis*. 2014;14:187.
102. Kitagawa H, Mori M, Kashiyama S, Sasabe Y, Ukon K, Shimokawa N, et al. Effect of pulsed xenon ultraviolet disinfection on methicillin-resistant *Staphylococcus aureus* contamination of high-touch surfaces in a Japanese hospital. *Am J Infect Control*. 2020;48(2):139–42.
103. Stibich M, Stachowiak J, Tanner B, Berkheiser M, Moore L, Raad I, et al. Evaluation of a pulsed-xenon ultraviolet room disinfection device for impact on hospital operations and microbial reduction. *Infect Control Hosp Epidemiol*. 2011;32(3):286–8.
104. Kitagawa H, Tadera K, Mori M, Kashiyama S, Nomura T, Omori K, et al. The effect of pulsed-xenon ultraviolet disinfection on surfaces contaminated with vancomycin-resistant Enterococci in a Japanese hospital. *J Infect Chemother*. 2021;27(11):1665–8. <https://doi.org/10.1016/j.jiac.2021.08.011>.
105. Ghantaji SS, Stibich M, Stachowiak J, Cantu S, Adachi JA, Raad II, et al. Non-inferiority of pulsed xenon UV light versus bleach for reducing environmental *Clostridium difficile* contamination on high-touch surfaces in *Clostridium difficile* infection isolation rooms. *J Med Microbiol*. 2015;64(Pt 2):191.
106. Kitagawa H, Mori M, Hara T, Kashiyama S, Shigemoto N, Ohge H. Effectiveness of pulsed xenon ultraviolet disinfection for *Clostridioides* (*Clostridium*) *difficile* surface contamination in a Japanese hospital. *Am J Infect Control*. 2021;49(1):55–8.
107. Haas JP, Menz J, Dusza S, Montecalvo MA. Implementation and impact of ultraviolet environmental disinfection in an acute care setting. *Am J Infect Control*. 2014;42(6):586–90.
108. Levin J, Riley LS, Parrish C, English D, Ahn S. The effect of portable pulsed xenon ultraviolet light after terminal cleaning on hospital-associated *Clostridium difficile* infection in a community hospital. *Am J Infect Control*. 2013;41(8):746–8.
109. Falagas ME, Thomaidis PC, Kotsantis IK, Sgouros K, Samonis G, Karageorgopoulos DE. Airborne hydrogen peroxide for disinfection of the hospital environment and infection control: a systematic review. *J Hosp Infect*. 2011;78(3):171–7.
110. Weber DJ, Rutala WA, Anderson DJ, Chen LF, Sickbert-Bennett EE, Boyce JM. Effectiveness of ultraviolet devices and hydrogen peroxide systems for terminal room decontamination: focus on clinical trials. *Am J Infect Control*. 2016;44(5 Suppl):e77–84.
111. Dong Z, Zhou N, Liu G, Zhao L. Role of pulsed-xenon ultraviolet light in reducing healthcare-associated infections: a systematic review and meta-analysis. *Epidemiol Infect*. 2020;148:e165.
112. Ramos CCR, Roque JLA, Sarmiento DB, Suarez LEG, Sunio JTP, Tabungar KIB, et al. Use of ultraviolet-C in environmental sterilization in hospitals: a systematic review on efficacy and safety. *Int J Health Sci (Qassim)*. 2020;14(6):52–65.
113. World Health Organisation (WHO). Antimicrobial resistance 2020 [Available from: <https://www.who.int/news-room/fact-sheets/detail/antimicrobial-resistance>].
114. Klein EY, Tseng KK, Pant S, Laxminarayan R. Tracking global trends in the effectiveness of antibiotic therapy using the drug resistance index. *BMJ Glob Health*. 2019;4(2):e001315.
115. European Center for Disease Prevention and Control (ECDC). Surveillance atlas of infectious disease 2019 [Available from: <https://atlas.ecdc.europa.eu/public/index.aspx?Dataset=27&HealthTopic=4>].
116. Bartels MD, Kristoffersen K, Slotsbjerg T, Rohde SM, Lundgren B, Westh H. Environmental methicillin-resistant *Staphylococcus aureus* (MRSA) disinfection using dry-mist-generated hydrogen peroxide. *J Hosp Infect*. 2008;70(1):35–41.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Ready to submit your research? Choose BMC and benefit from:

- fast, convenient online submission
- thorough peer review by experienced researchers in your field
- rapid publication on acceptance
- support for research data, including large and complex data types
- gold Open Access which fosters wider collaboration and increased citations
- maximum visibility for your research: over 100M website views per year

At BMC, research is always in progress.

Learn more biomedcentral.com/submissions

